

NEW RESEARCH PAPERS

Infarct-Related Ventricular Tachycardia

Redefining the Electrophysiological Substrate of the Isthmus During Sinus Rhythm



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CME/MOC Objective for This Article: Upon completion of this activity, the learner should be able to: 1) Describe the electrophysiological substrate during sinus rhythm of infarct-related ventricular tachycardia in terms of vulnerability for re-entry; 2) evaluate the substrate of patients with infarct-related ventricular tachycardia for areas with slow conduction that are vulnerable for unidirectional block and re-entry; and 3) for those patients with infarct-related ventricular tachycardia, target those areas with slow conduction that are vulnerable for re-entry and can support tachycardias of multiple morphologies.

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ABSTRACT

OBJECTIVES In this study, the scientific objective was to characterize the electrophysiological substrate of the ventricular tachycardia (VT) isthmus during sinus rhythm.

BACKGROUND The authors have recently described the electrophysiological characteristics of the VT isthmus using a novel in vivo high-resolution mapping technology.

METHODS Sixteen swine with healed infarction were studied using high-resolution mapping technology (Rhythmia, Boston Scientific, Cambridge, Massachusetts) in a closed-chest model. The left ventricle was mapped during sinus rhythm and analyzed for activation, conduction velocity, electrogram shape, and amplitude. Twenty-four VTs allowed detailed mapping of the common-channel "isthmus," including the "critical zone." This was defined as the zone of maximal conduction velocity slowing in the circuit, often occurring at entrance and exit from the isthmus caused by rapid angular change in activation vectors.

RESULTS The VT isthmus corresponded to sites displaying steep activation gradient (SAG) during sinus rhythm with conduction velocity slowing of $58.5 \pm 22.4\%$ (positive predictive value [PPV] 60%). The VT critical zone displayed SAG with greater conduction velocity slowing of $68.6 \pm 18.2\%$ (PPV 70%). Critical-zone sites were consistently localized in areas with bipolar voltage ≤ 0.55 mV, whereas isthmus sites were localized in areas with variable voltage amplitude (1.05 ± 0.80 mV [0.03 to 2.88 mV]). Importantly, critical zones served as common-site "anchors" for multiple VT configurations and cycle lengths. Isthmus and critical-zone sites occupied only $18.0 \pm 7.0\%$ of the low-voltage area (≤ 1.50 mV). Isolated late potentials were present in both isthmus and nonisthmus sites, including dead-end pathways (PPV 36%; 95% confidence interval: 34.2% to 39.6%).

CONCLUSIONS The VT critical zone corresponds to a location characterized by SAG and very low voltage amplitude during sinus rhythm. Thus, it allows identification of a re-entry anchor with high sensitivity and specificity. By contrast, voltage and electrogram characteristics during sinus rhythm have limited specificity for identifying the VT isthmus. (J Am Coll Cardiol EP 2018;4:1033-48) © 2018 by the American College of Cardiology Foundation.

Activation mapping of ventricular tachycardia (VT) is the gold-standard method for description of the re-entrant circuit and identification of its isthmus. However, activation mapping is limited by hemodynamic nontolerance and relatively low temporal and spatial resolution. Substrate mapping has been used as an alternative method to identify the isthmus of post-infarction VT during sinus

rhythm (1-6). The principle underlying substrate mapping is that bundles of surviving myocytes within heterogeneous scar identified during sinus rhythm may form isthmuses during VT. This has led to the widespread use of voltage mapping to identify channels of viable myocardium, pace-mapping techniques aimed to produce a QRS morphology similar to the VT, and identification of abnormal electrograms

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All authors attest they are in compliance with human studies committees and animal welfare regulations of the authors' institutions and Food and Drug Administration guidelines, including patient consent where appropriate. For more information, visit the *JACC: Clinical Electrophysiology* [author instructions page](#).

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(EGMs) (i.e., fractionated, late potentials) thought to represent the VT isthmus (7,8). Despite this approach, current substrate-mapping techniques have limited specificity for identifying the VT isthmus during sinus rhythm (9). It is therefore not surprising that confined ablation strategies guided by current substrate mapping techniques are less effective than extensive ablation strategies directed in eliminating all viable myocardium in and around the infarct (i.e., substrate homogenization) (10-15). This underlies the limitations of current substrate-mapping techniques to specifically identify the electrophysiologic substrate: the specific zone(s) in and around the infarct, capable of supporting re-entry and VT.

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A major limitation of current substrate-mapping techniques relates to oversimplification of the relationship between the VT circuit and the underlying substrate. In particular, it assumes that the substrate for re-entry in patients with healed infarction is purely structural, neglecting the electrophysiological properties responsible for initiation and perpetuation of re-entry. These have been studied in detail and include slow conduction due to cellular uncoupling and nonuniform anisotropic conduction and dispersion of refractoriness with nonuniform recovery of excitability (16). Fundamental work in a canine model of healed infarction showed that isthmuses of different VTs often share one common region and that this region can be identified during sinus rhythm as an area with steep conduction slowing (17). However, these studies required detailed EGM recordings from a multielectrode array placed on the epicardial surface, limiting its applicability to humans.

Recent advancements in mapping technology approved for use in human provide an opportunity to examine the electrophysiological properties of VT in greater detail. We have recently described the electrophysiological properties of the post-infarction VT circuit using high-resolution mapping technology (Rhythmia, Boston Scientific, Marlborough, Massachusetts) (18). In this report, we describe the structural and functional properties of the VT isthmus during sinus rhythm. In particular, we compare these properties to non-isthmus sites in attempt to better characterize the *arrhythmogenic substrate* of infarct-related VT.

METHODS

SWINE INFARCT MODEL. We studied 16 swine with chronic anterior wall infarction. Our swine model has been described previously and closely

approximates human infarction with re-entrant VT (19). In brief, Yorkshire swine (male, 35 kg to 40 kg) underwent selective balloon occlusion of the left anterior descending artery for duration of 180 min. After 8 to 10 weeks, animals underwent electrophysiology study, including mapping during sinus rhythm and VT, as described subsequently. This research was performed at the Beth Israel Deaconess Medical Center, Harvard Medical School, Boston, Massachusetts. The Institutional Animal Care and Use Committee approved this research protocol.

ELECTROPHYSIOLOGY STUDY. The electrophysiology study was performed under general anesthesia with isoflurane inhalation. A pentapolar catheter (Bard EP, Lowell, Massachusetts) was placed in the right ventricular apex (RVA) to allow pacing and to act as an intracardiac activation reference. The proximal electrode was positioned in the inferior vena cava and served as an indifferent unipolar electrode. The left ventricle (LV) was initially mapped during sinus rhythm and then during VT as described subsequently. Induction of VT was performed using programmed stimulation from the RVA at a current strength twice the capture threshold and a pulse width of 2.0 ms. Stimulation was performed at paced cycle lengths of 600 and 400 ms with 1 to 4 extrastimuli down to ventricular effective refractory period. If electrical stimulation from the RVA failed to induce VT, stimulation was repeated from the right ventricular outflow tract, followed by the LV. We attempted to map all sustained monomorphic VTs. If the VT was not hemodynamically tolerated, it was terminated by pacing or electrical cardioversion. In these cases, vasopressor support (phenylephrine bolus of 100 to 500 μ g) was administered to increase the blood pressure before the next attempt of induction.

LV MAPPING DURING SINUS RHYTHM. Mapping of the LV was performed during sinus rhythm (heart rate range 80 to 110 beats/min) using the Rhythmia mapping system including its proprietary Orion 64-electrode basket catheter (Boston Scientific, Cambridge, Massachusetts) (20). The length of the basket is 23 mm, and its nominal diameter is 18 mm. The surface area of each electrode is 0.4 mm², and the distance between electrodes is 2.5 mm from center to center. The catheter was introduced into the LV via a percutaneous transaortic approach, and mapping of the chamber was performed by slowly navigating the steerable basket catheter throughout

ABBREVIATIONS AND ACRONYMS

EGM = electrogram

LAVA = local abnormal
ventricular activity

LV = left ventricle

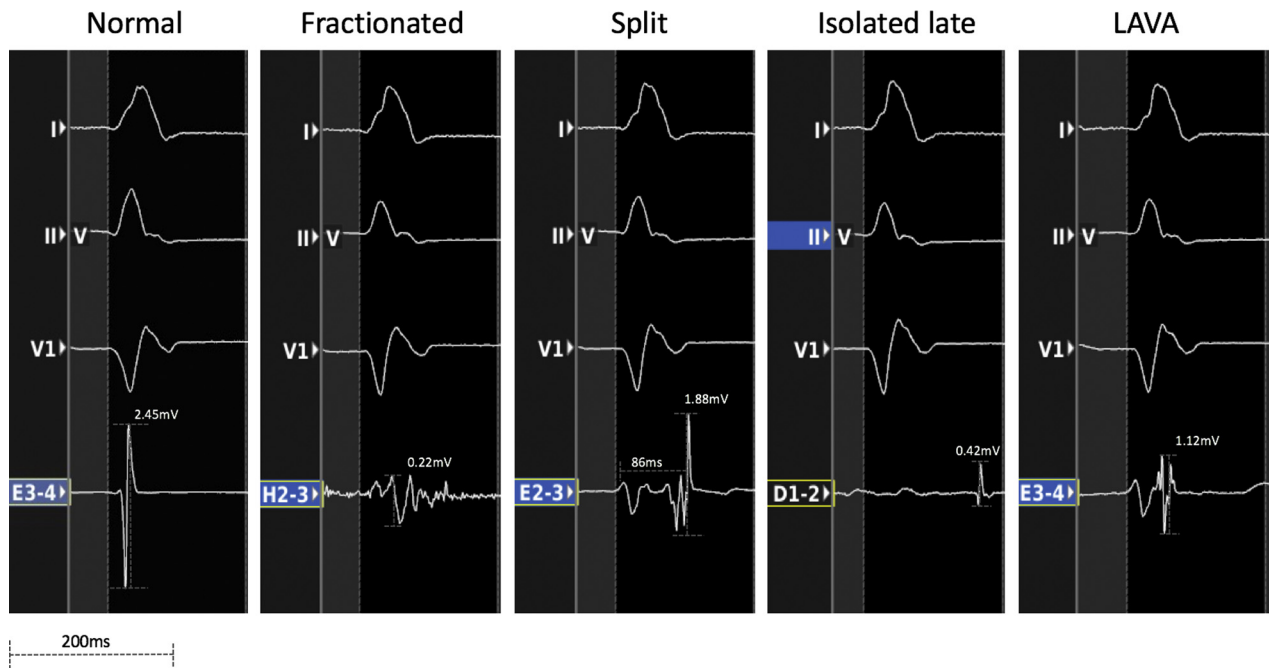
NPV = negative predictive
value

PPV = positive predictive value

RVA = right ventricular apex

SAG = steep activation
gradient

VT = ventricular tachycardia

FIGURE 1 Classification of Electrograms

Electrograms (EGMs) were classified using basic descriptors as normal, fractionated low-amplitude, split, and isolated late potentials. EGMs were also classified as local abnormal ventricular activity (LAVA) or non-LAVA. Please see text for details.

the entire chamber. We attempted to include only data points in contact with the endocardial surface. This included: 1) near-field EGM with similar morphology ≥ 2 consecutive beats; 2) points within 2 mm from the outmost surface as determined following completion of the map; and 3) real-time imaging of the basket catheter by intracardiac echocardiography catheter (AcuNav, Biosense Webster Inc., Diamond Bar, California). The final number of points represents the sum of all data points acquired at different beats during controlled navigation of the basket catheter in the chamber. A requisite for a complete map was a mapping density with a fill threshold ≤ 2 mm, limiting interpolation between points to < 2 mm.

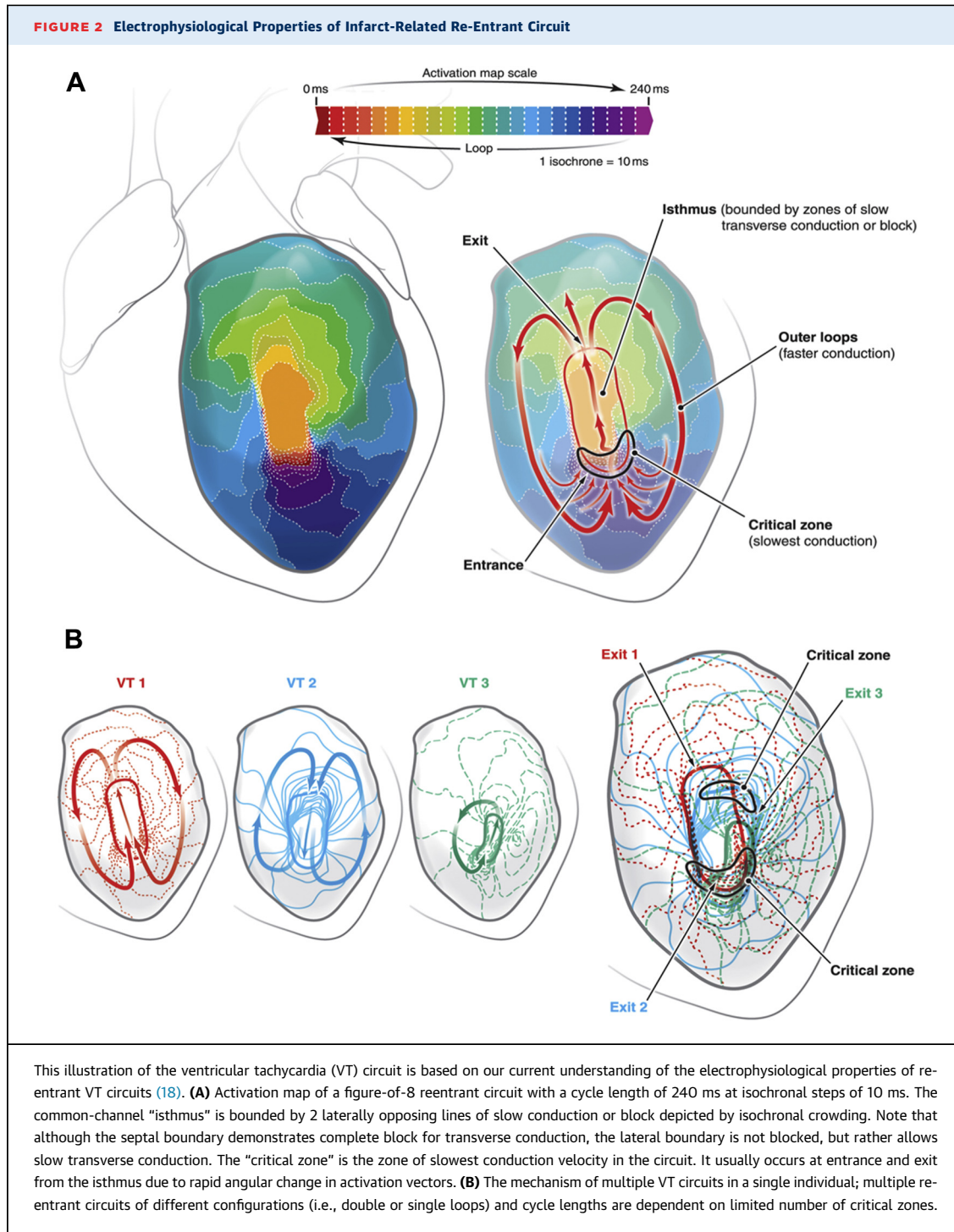
RECORDING AND ANALYSIS OF EGMs. The bandpass of filtered EGMs ranged from 30 to 300 Hz (bipolar signals) and 1 to 300 Hz (unipolar signals). The reference (negative) input of the unipolar EGM was an electrode positioned in the inferior vena cava. Selected EGMs had minimum bipolar voltage amplitudes of 0.03 mV (2-fold higher than the noise level in our laboratory). All EGMs were reviewed offline at a sweep speed of 200 to 400 mm/s. Data points were included for analysis only if ≥ 2 consecutive beats had similar and

distinct near-field EGM morphology and stable activation timing (± 2 ms).

Unipolar EGMs were used to measure local activation time (at minimal $-dV/dt$). At sites with multi-component or fractionated EGMs, differentiation between near-field (“local”) and far-field (“remote”) potentials is often difficult. In these multicomponent EGMs, the local potential (or potentials) often originates from a relatively small mass of myocardial bundles within scar, whereas the remote potential is often generated by a larger mass of surrounding cardiomyocytes that may generate a more negative dV/dt value, misleading automated EGM annotation algorithms. We analyzed multicomponent EGMs using a method we developed to better differentiate near-field from far-field EGMs. In principle, local potentials conduct within tissue to exhibit a spatiotemporal pattern of propagation, whereas remote potentials generated by the sum (average) of the surrounding EGMs do not exhibit a spatiotemporal pattern of propagation (Online Figure 1).

EGMs were classified according to the following basic descriptors:

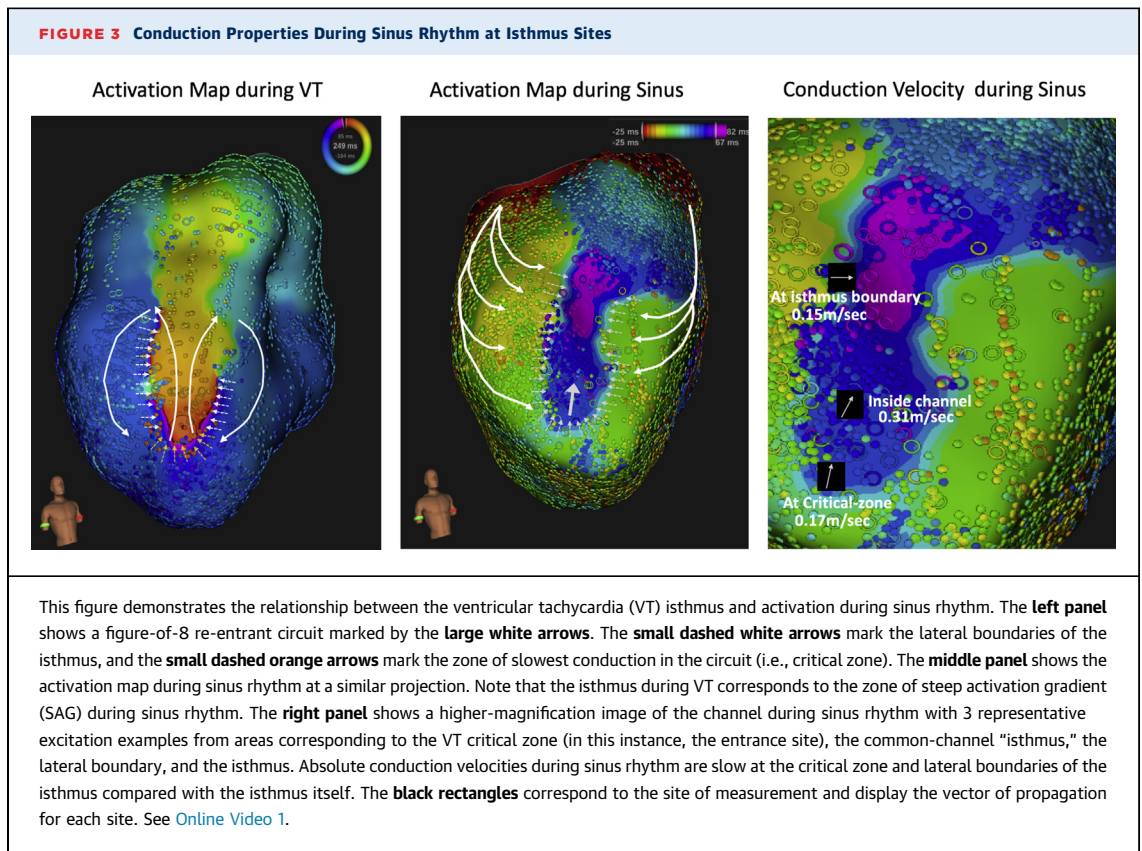
1. Normal EGMs: Voltage amplitude ≥ 1.50 mV, signals with ≤ 3 intrinsic deflections, duration ≤ 70 ms.



These criteria have been specifically validated for the Rhythmia mapping system and its mapping catheter (21).

2. Fractionated Low-Amplitude EGMs: Signals with multiple (≥ 5) intrinsic deflections, amplitude < 0.50 mV, duration ≥ 133 ms (22).

3. Split EGMs: Signals with double or multiple components (irrespective of voltage amplitude) separated by an isoelectric interval or a period of very low-amplitude signals of ≥ 50 -ms duration, occurring during the surface QRS or within 50 ms after its completion.



4. Isolated Late EGMs: Local high-frequency signals (distinct from far field components), often of low amplitude, occurring ≥ 50 ms after the QRS.
5. Nonclassified EGMs: EGMs not fitting into categories 1 to 4.

In addition to the previously mentioned classification, EGMs were also classified as local abnormal ventricular activity (LAVA). LAVA is a composite EGM, defined as sharp high-frequency potentials, possibly of low amplitude, distinct from a far-field ventricular EGM occurring any time during or after the far-field ventricular EGM (23). As LAVA is commonly used to guide substrate-based VT ablation, we examined its sensitivity and specificity for the VT isthmus. Examples of normal and abnormal EGMs are shown in [Figure 1](#).

CONDUCTION VELOCITY DURING SINUS RHYTHM. Measurement of propagation velocity during sinus rhythm was calculated based on the activation time and the known distance between data points along a vector that has an origin and direction. Propagation velocities were calculated using MATLAB triangulation algorithm (24). Conduction block was defined as absolute conduction velocity ≤ 10 cm/s,

consistent with previous reports (25). Wavefront curvature was calculated using the streamline MATLAB algorithm (26). Detailed description is provided in the [Online Appendix](#). As absolute propagation velocities can vary among individuals, relative changes in propagation velocity were compared in reference to the maximal conduction velocity for each individual swine (defined as the 95th percentile).

Spatial changes in conduction velocity during sinus rhythm are described by gradients of activation. We defined steep activation gradient (SAG) as conduction velocity slowing of $\geq 50\%$ that occurs over a longitudinal length ≤ 5 mm. The sensitivity and specificity of SAG during sinus rhythm to identify the VT isthmus and the critical zone was calculated separately for conduction velocity slowing $\geq 50\%$ and for conduction velocity slowing $\geq 75\%$.

VOLTAGE AND ACTIVATION DURING SINUS RHYTHM. Bipolar voltage maps are displayed using a color scale from red to purple; red represents low voltage, and purple represents high voltage. The cutoff for normal voltage was 1.50 mV, as previously reported for this mapping system and catheter (21). Unipolar or bipolar

TABLE 1 Sensitivity, Specificity, and Predictive Value of Sinus Parameters for the VT Isthmus

	Sensitivity	Specificity	PPV	NPV
Voltage abnormality (≤ 1.5 mV)				
Isthmus	72.2 (68.1-76.4)	55.6 (53.4-58.7)	24.0 (21.8-27.6)	90.2 (88.6-96.4)
Critical zone	100.0	43.2 (38.5-48.8)	21.0 (17.7-25.3)	100.0
EGM abnormality				
Isthmus				
Split EGMs	48.0 (44.8-53.2)	64.0 (61.2-68.4)	48.0 (46.2-51.3)	90.0 (87.2-93.6)
Fractionated low-amplitude EGMs	22.0 (19.1-25.8)	33.0 (29.7-36.4)	28.0 (25.4-32.1)	82.0 (78.8-85.4)
Isolated late EGMs	16.0 (14.1-19.2)	68.0 (64.4-71.3)	36.0 (34.2-39.6)	88.0 (84.6-91.4)
LAVA	82.0 (78.8-85.4)	38.0 (35.4-42.2)	31.0 (27.2-35.7)	90.0 (86.6-94.1)
Critical zone				
Split EGMs	68.0 (65.1-71.8)	69.0 (67.1-72.5)	46.0 (44.4-48.3)	94.0 (90.3-97.1)
Fractionated low-amplitude EGMs	25.0 (21.1-27.7)	32.0 (30.1-35.4)	22.0 (19.6-24.6)	88.0 (83.8-91.5)
Isolated late EGMs	4.0 (3.1-6.4)	28.0 (26.2-30.5)	16.0 (13.6-19.1)	80.0 (78.2-83.7)
LAVA	86.0 (83.4-89.2)	32.0 (28.8-36.4)	14.0 (11.5-18.7)	96.0 (92.5-98.8)
Conduction velocity slowing				
Isthmus				
Conduction velocity slowing $\geq 50\%$	80.0 (78.5-83.1)	73.0 (70.2-76.3)	54.0 (51.3-58.2)	96.0 (94.6-98.6)
Conduction velocity slowing $\geq 75\%$	72.0 (69.3-75.6)	80.0 (77.5-83.7)	60.0 (58.2-63.6)	94.0 (92.2-96.7)
Critical zone				
Conduction velocity slowing $\geq 50\%$	92.0 (88.6-95.2)	68.0 (65.2-74.3)	66.0 (63.4-69.1)	98.0 (95.6-99.5)
Conduction velocity slowing $\geq 75\%$	86.0 (84.6-90.3)	80.0 (78.1-84.2)	70.0 (68.8-74.6)	98.0 (96.2-99.2)

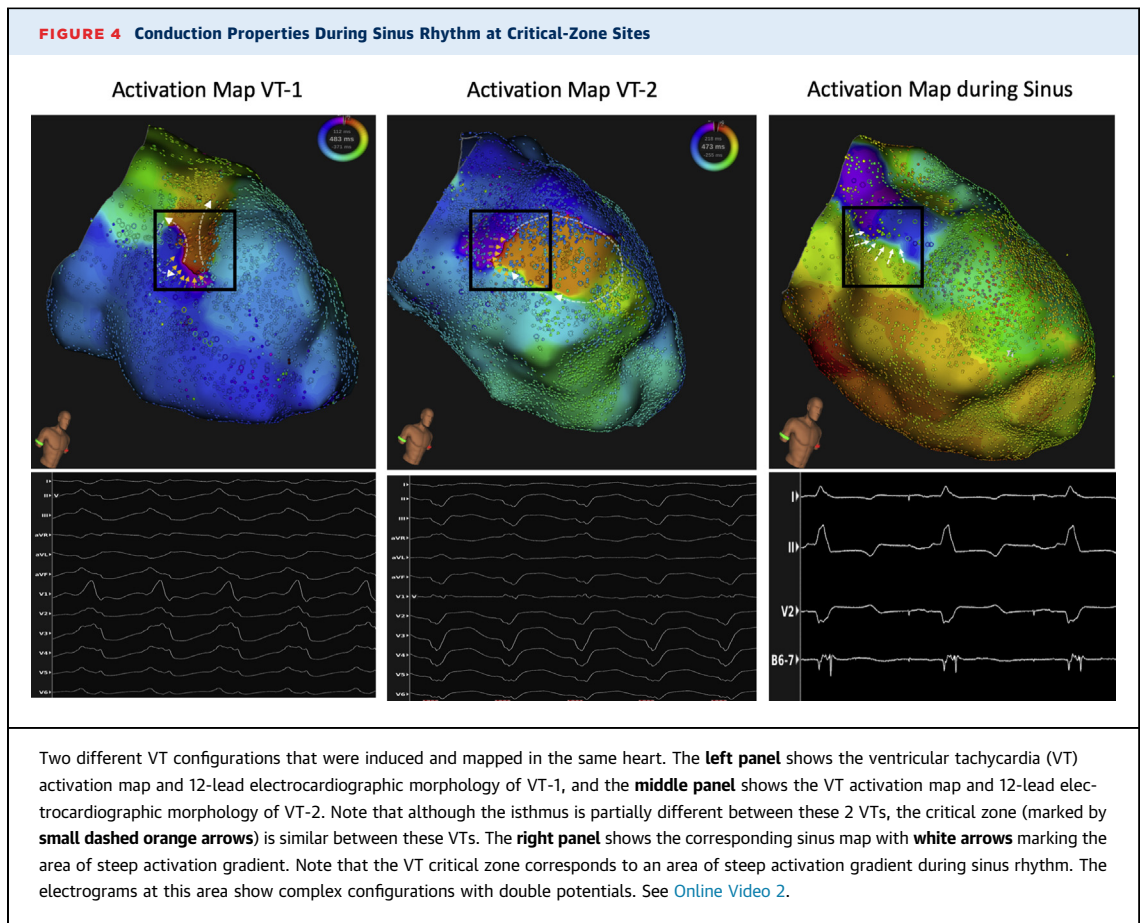
EGM = electrogram; LAVA = local abnormal ventricular activity; NPV = negative predictive value; PPV = positive predictive value; VT = ventricular tachycardia.

activation maps are displayed using isochrones drawn at 10-ms intervals and colored on a scale from red to purple.

ACTIVATION MAPPING OF VT. We have recently described our method for activation mapping of the VT circuit (18). In brief, mapping of a macro re-entrant VT was considered complete when: 1) $\geq 90\%$ of the tachycardia cycle length was mapped; 2) an isthmus “common-channel” was identified; and 3) mapping density at zones of slow conduction was adequate, limiting data interpolation between points to ≤ 3 mm. Macro re-entrant circuits had a well-defined entrance site, a common channel, and a distinct exit site. The “entrance” was defined as the site at which the orthodromic wavefront enters a “common channel.” The “isthmus” was defined as a channel bounded by 2 lateral lines of block (or slow conduction), producing an orthodromic wavefront. The “exit” was defined as the site at which the orthodromic wavefront exits the common channel to activate the remainder of the ventricle. In addition, we also defined the “critical zone” as the zone of slowest conduction velocity in the VT circuit, as we reported previously (18). This most commonly occurs at entrance or exit from the isthmus because of rapid angular change in activation vectors. Figure 2 shows a schematic illustration

of the VT circuit, including the isthmus and critical zone.

STATISTICAL ANALYSIS. Continuous variables with normal distribution are reported as mean \pm SD. For those with non-normal distribution, range and median are reported. For comparisons of continuous variables, a Student paired *t* test was used if data were normally distributed and a signed rank test was used for non-normally distributed variables. Numerical data are given as mean \pm SD (range, median). The sensitivity, specificity, positive predictive value (PPV), and negative predictive value (NPV) of EGM characteristics (normal, fractionated low amplitude, split, late, and LAVA) and conduction properties during sinus rhythm to identify the isthmus were estimated using a 2-stage method. In the first stage, we fitted generalized linear mixed-effects models in which each pig was treated as a random effect (in reference to EGMs). In this stage, we treated the event (VT isthmus) as the outcome and predictor as the independent variable (for PPV and NPV) and then switched their roles (for sensitivity and specificity). In the second stage, we used the estimated model parameters to compute the corresponding accuracy parameter by integrating out the random effect. A *p* value < 0.05 was considered statistically significant. Interobserver and intraobserver variability in EGM



classification was quantified using the kappa statistic, which measures agreement between observers while accounting for chance. Analyses were conducted using STATA release 13 (StataCorp, College Station, Texas).

RESULTS

In 16 swine with healed infarction, endocardial map of the LV was performed during sinus rhythm. The number of data points per LV sinus map was $12,860 \pm 3,172$ (range 8,932 to 18,992; median 13,024). In these swine, VT activation maps were also performed, providing the basis for evaluation of the VT isthmus and critical zone during sinus rhythm.

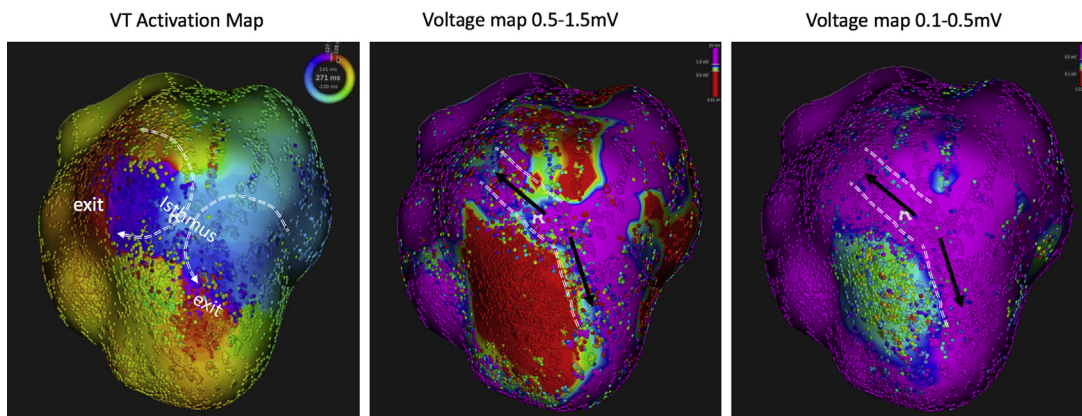
VT CHARACTERISTICS. The electrophysiological characteristics of these VTs have been previously reported and were needed in this study for comparison with the electrical behavior during sinus rhythm (18). A total of 24 sustained monomorphic VTs with tachycardia cycle length of 302 ± 65 ms (range: 237 to

488 ms; median 273 ms) were mapped in 16 swine. As shown in [Figure 2](#), these circuits exhibited an entrance site, a common channel with diastolic activity, and a separate exit site whose activation encompassed the tachycardia cycle length. The critical zone occurred most commonly at entrance sites (66.7%; 16 of 24 VTs), followed by exit sites (20.8%; 5 of 24 VTs), and isthmus sites (12.5%; 3 of 24 VTs). The number of activation data points per VT map was $7,642 \pm 4,228$ (range: 2,302 to 21,118; median 7,580), and the number of activation points within the isthmus, including the critical zone, was 313 ± 114 (range: 121 to 488; median 302). Overall, the number of data points collected during VT was smaller than the number of data points collected during sinus rhythm ($p < 0.001$).

CONDUCTION PROPERTIES DURING SINUS RHYTHM AT ISTHMUS SITES

Local endocardial conduction velocities in the ventricle during sinus rhythm had nonhomogenous distribution, exhibiting various degrees of

FIGURE 5 Relationship Between the VT Isthmus and Voltage Amplitude During Sinus Rhythm



The **left panel** shows an example of a complex Y-configuration re-entrant ventricular tachycardia (VT) circuit with 2 exits (tachycardia cycle length of 271 ms). The **middle and right panels** show the corresponding bipolar voltage maps during sinus rhythm at scales of 0.50 to 1.50 mV and 0.10 to 0.50 mV, respectively. Note that voltage amplitude is higher at the common-channel (“isthmus”) compared with its lateral boundary.

conduction velocity slowing in and around the infarct zone. Absolute conduction velocities in the infarct and peri-infarct zone ranged from ≤ 10 cm/s in areas of conduction block to 88 cm/s in healthy myocardium and conduction bundles.

ISTHMUS SITES. Conduction velocity during sinus rhythm at isthmus sites was $41.5 \pm 17.1\%$ (range: 38.2% to 100%) of the maximal conduction velocity. The VT isthmus sites hosted zones displaying SAG, including conduction block during sinus rhythm. **Figure 3** shows an activation map during VT with the corresponding activation map during sinus rhythm. This shows that the VT isthmus corresponded to an area of SAG with significant conduction slowing during sinus rhythm. **Online Video 1** shows the corresponding propagation maps during VT and sinus rhythm.

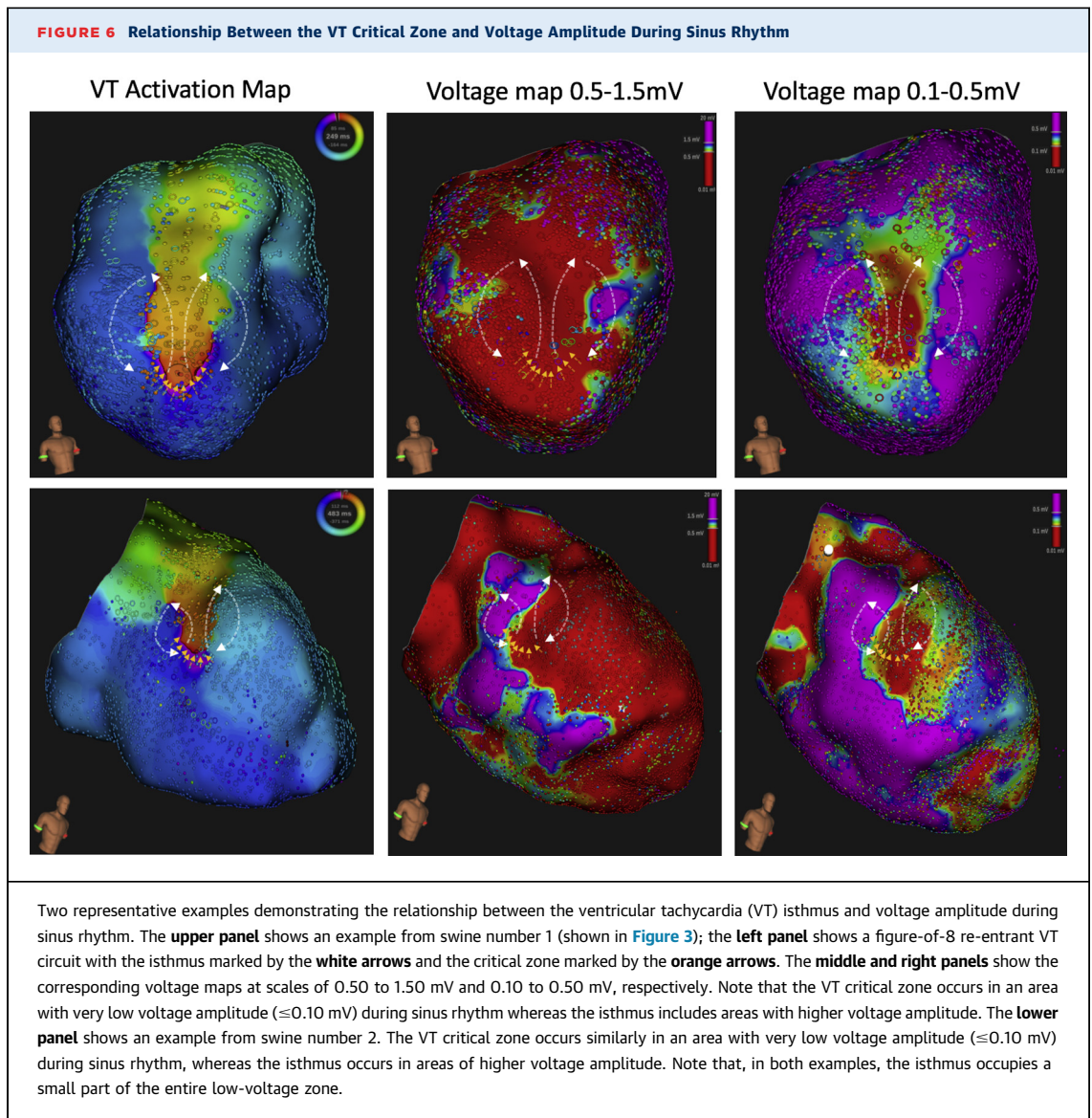
Although the VT isthmus corresponded to sites hosting conduction velocity slowing during sinus rhythm, conduction block was evident in only 37.5% (range: 22% to 67.0%) of the total isthmus length. This suggests that the VT isthmus is partially fixed and largely functional. The sensitivity, specificity, and PPV of SAG $\geq 50\%$ during sinus rhythm to detect the VT isthmus was 80.0% (range: 78.5% to 83.1%), 73.0% (range: 70.2% to 76.3%), and 54.0% (range: 51.3% to 58.2%), respectively. The sensitivity, specificity, and PPV of SAG $\geq 75\%$ to detect the VT isthmus was 72.0% (range: 69.3% to 75.6%), 80.0% (range: 77.5% to 83.7%), and 60.0% (range: 58.2% to 63.6%), respectively.

CRITICAL-ZONE SITES. Conduction velocity during sinus rhythm was slower at critical-zone sites

compared with isthmus sites ($31.4 \pm 12.2\%$ [range: 28.2% to 35.4%] vs. $41.5 \pm 17.1\%$ [range: 38.2% to 100%] of the maximal conduction velocity; $p = 0.001$). The sensitivity, specificity, and PPV of SAG $\geq 50\%$ during sinus rhythm to identify the critical zone was 92.0% (88.6% to 95.2), 68.0% (range: 65.2% to 74.3%) and 66.0% (range: 63.4% to 69.1%), respectively. The sensitivity, specificity, and PPV of conduction velocity slowing $\geq 75\%$ during sinus rhythm to identify the critical zone were 86.0% (range: 84.6% to 90.3%), 80.0% (range: 78.1% to 84.2%), and 70.0% (range: 68.8% to 74.6%), respectively. **Table 1** includes sensitivity, specificity, PPV, and NPV of conduction velocity slowing for isthmus and critical-zone sites.

DIFFERENT VT MORPHOLOGIES ASSOCIATED WITH CIRCUITS IN THE SAME AREA OF THE CRITICAL ZONE.

The critical-zone site was common to multiple VT configurations, exhibiting variable configurations and cycle lengths in the same heart. In 7 of 16 hearts with sustained VT, tachycardias with more than 1 morphology were induced and mapped (2.14 ± 0.30 ; median 2.00). In 3 hearts, different QRS morphologies were associated with re-entrant wavefronts moving in opposite directions around the same critical zone. In 3 hearts, different VT configurations were associated with re-entrant wavefronts moving in the same direction around the same critical zone, but there were small changes in the extent of the line of block that resulted in different exit sites. In 1 heart, re-entrant circuits at different sites caused different morphologies. **Figure 4** shows an example of 2



different tachycardias occurring in the same heart and sharing a similar critical zone. [Online Video 2](#) shows the corresponding propagation map during VT and sinus rhythm.

VOLTAGE DISTRIBUTION DURING SINUS RHYTHM AT ISTHMUS AND CRITICAL-ZONE SITES

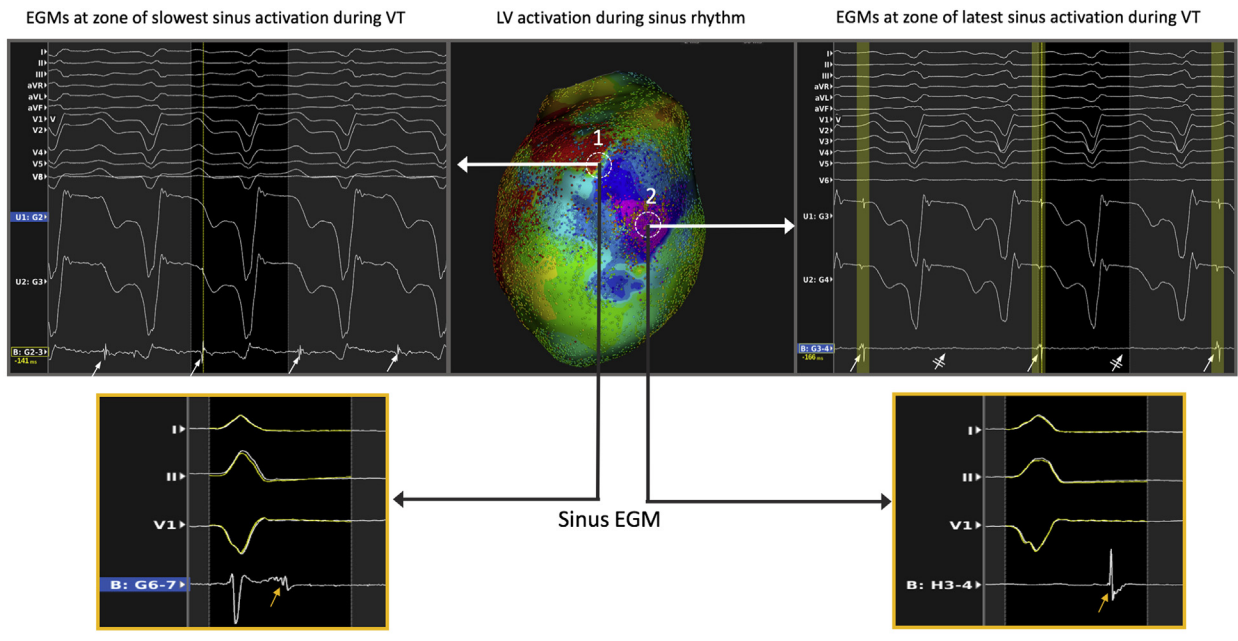
ISTHMUS SITES. The bipolar voltage amplitude at isthmus sites during sinus rhythm was variable and ranged from low to normal (1.05 ± 0.80 mV [range: 0.03 to 2.88 mV; median 1.00 mV]). The voltage amplitude was higher in the common channel compared with its lateral boundaries (1.25 ± 0.32 mV

[range: 0.08 to 2.88 mV] vs. 0.68 ± 0.25 mV [range: 0.03 to 1.82 mV]; $p < 0.001$). [Figure 5](#) shows an example of typical voltage distribution in isthmus sites with higher amplitude in the common channel compared with its lateral boundaries.

CRITICAL-ZONE SITES. Critical zones were consistently localized in areas with bipolar voltage amplitude ≤ 0.55 mV. The bipolar amplitude at critical-zone sites was 0.22 ± 0.30 mV (range: 0.03 to 0.55 mV; median 0.21 mV). [Figure 6](#) shows representative examples of voltage distribution during sinus rhythm at isthmus and critical-zone sites.

The VT isthmus including the critical-zone occupied only $18 \pm 7\%$ (range: 9% to 32%; median 19%) of

FIGURE 7 Relationship Between Isthmus Sites and Sites of Latest Activation During Sinus Rhythm



This figure shows a left ventricular (LV) activation map during sinus rhythm in a swine with healed anterior-wall infarction (**middle panel**). The **red color** represents early activation, and the **purple color** represents the latest activation. Note that the area of steep activation gradient and conduction velocity slowing during sinus rhythm (labeled "1") corresponds to the isthmus during ventricular tachycardia (VT), as shown by the presence of mid-diastolic potentials (**left panel**). In contrast, the area of latest activation during sinus rhythm (**right panel**) exhibits 2:1 block during VT (**white arrows**). The electrograms (EGMs) during sinus rhythm at the area of steep activation gradient exhibit fractionated low amplitude potentials (**orange arrow**), whereas EGMs during sinus rhythm at the area of latest activation exhibit isolated late potentials.

the entire low low-voltage area. Moreover, the ratio between the isthmus(s) to low-voltage area was similar between hearts with 1 VT and hearts with multiple VTs ($17 \pm 6\%$ vs. $20 \pm 9\%$; $p = 0.15$). This is because multiple VTs in each heart often originated from a limited area. Overall, the sensitivity, specificity, PPVs, and NPVs of voltage abnormality for identification of isthmus and critical zones were lower in comparison with abnormalities in conduction properties (**Table 1**).

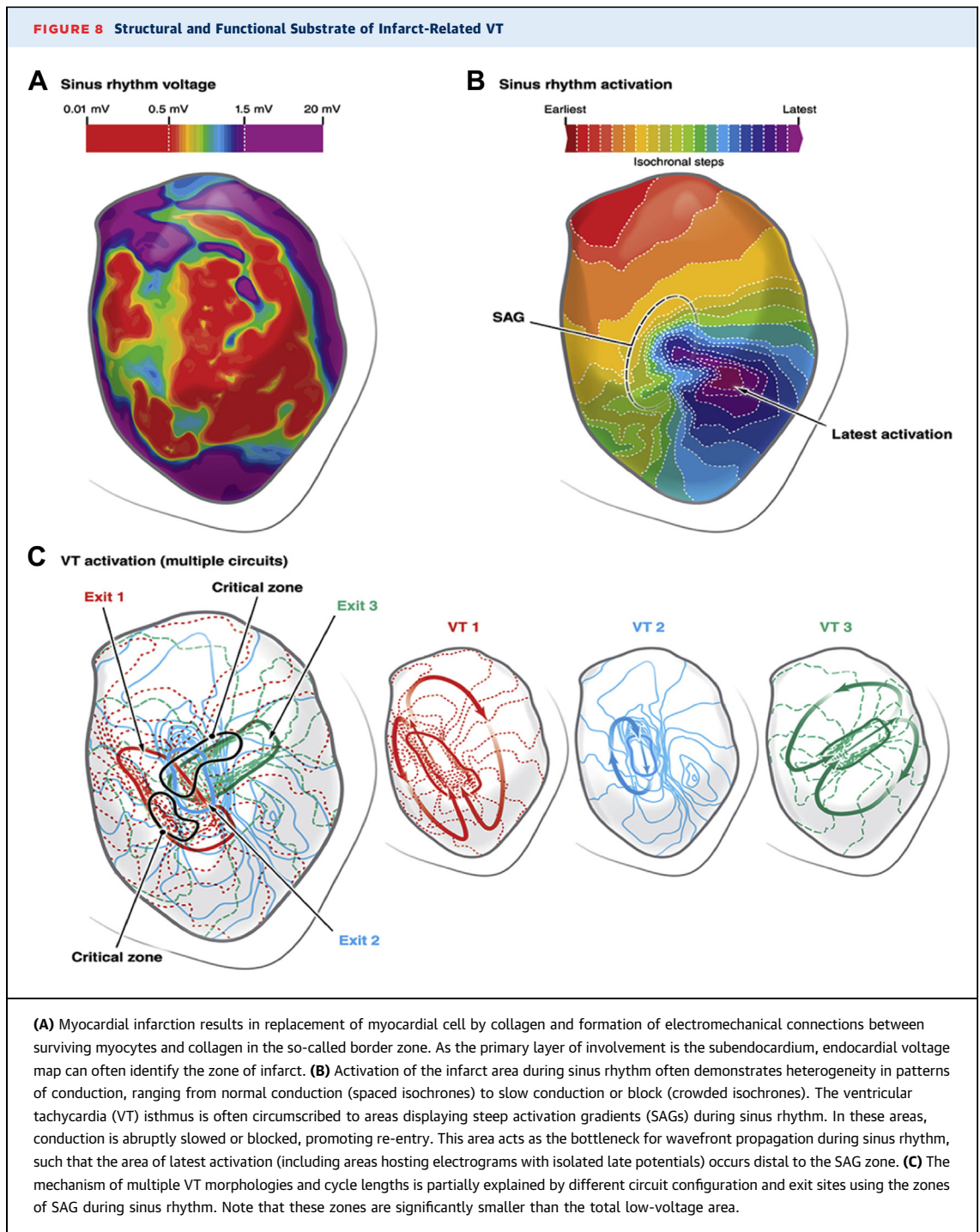
EGM CONFIGURATION DURING SINUS RHYTHM AT ISTHMUS SITES

The frequency and type of EGMs during sinus rhythm were compared between isthmus (including critical zone) and nonisthmus sites. The intraobserver and interobserver variability was good, with kappa values of 0.821 and 0.716, respectively.

ISTHMUS SITES. Split EGMs were the most frequent abnormal EGM type in isthmus sites, constituting

$48 \pm 13\%$ of the EGMs present in isthmus sites. Fractionated low-amplitude EGMs were also frequent ($22 \pm 8\%$). Split and low-amplitude fractionated EGMs were also present in nonisthmus sites, such that their specificity for isthmus sites was 64.0% (range: 61.2% to 68.4%) and 33.0% (range: 29.7% to 36.4%), respectively. Isolated late EGMs were less frequent and constituted only $16 \pm 6\%$ of all isthmus EGMs. The specificity of isolated late potentials for isthmus sites was 68.0% (range: 64.4% to 71.3%). **Table 1** details the sensitivity, specificity, PPV, and NPV of EGM abnormalities for identification of isthmus sites.

CRITICAL-ZONE SITES. Split EGMs were also the most frequent abnormal EGM type in critical zones, constituting $68 \pm 12\%$ of all EGMs. In comparison with isthmus sites, critical-zone sites exhibited a higher frequency of split EGMs (68.0% [range: 65.1% to 71.8%] vs. 48.0% [range: 44.8% to 53.2%]; $p < 0.001$) and a lower frequency of isolated late EGMs (4.0% [range: 3.1% to 6.4%] vs. 16.0%



[range: 14.1% to 19.2%]; $p < 0.001$). This is consistent with higher frequency of slow conduction and block at critical-zone sites compared with isthmus sites.

In addition to classification of basic EGM types, we also measured the frequency of LAVA EGMs for

isthmus and critical-zone sites. LAVA was the most commonly recorded EGM at isthmus and critical-zone sites, constituting 82% (range: 78.8% to 85.4%) and 86% (range: 83.4% to 89.2%) of all EGMs, respectively. However, LAVA was also common in nonisthmus sites, such that the specificity of LAVA

for isthmus and critical-zone sites was only 38.0% (range: 43.5% to 55.4%) and 32.0% (range: 28.8% to 36.4%), respectively. **Table 1** details the sensitivity, specificity, PPV, and NPV of EGM abnormalities for identification of isthmus sites.

During sinus rhythm activation, the zones of SAG were uniformly proximal to the zones of latest ventricular activation, including the areas hosting EGMs with isolated late potentials. The SAG zones served as gateways for wavefront propagation into areas of later ventricular activation during sinus rhythm. Conduction velocity in areas of latest ventricular activation, including areas hosting isolated late potentials, was higher in comparison with SAG zones ($54.2 \pm 18.0\%$ [range: 49.5% to 60.4%] vs. $36.5 \pm 14.4\%$ [range: 28.2% to 50.0%] of maximal conduction velocity; $p < 0.001$). **Figure 7** shows the relationship between the VT isthmus and zones of SAG and late potentials during sinus rhythm.

Figure 8 summarizes the relationship among voltage abnormality, gradients of activation during sinus rhythm, and the VT isthmus, including the critical zone. The VT isthmus and critical zone(s) correspond to sites with SAG during sinus rhythm. In particular, critical zone(s) occur in sites of very low voltage amplitude and slow conduction (or block) during sinus rhythm. Multiple VT morphologies often occur because of re-entrant wavefronts rotating around the same critical zone in different directions or wavefronts rotating at similar directions but with small changes in the extent of the central line of block, resulting in different exit sites.

DISCUSSION

This study examined the electrophysiological characteristics of the VT isthmus during sinus rhythm in a swine model of healed infarction using a novel high-resolution mapping technology. We found that abnormal conduction properties during sinus rhythm showed a strong correspondence to the VT isthmus. By contrast, standard substrate mapping techniques including voltage and EGM abnormalities are sensitive but nonspecific for isthmus sites. Specifically:

1. The VT isthmus corresponded to sites hosting SAGs during sinus rhythm. In particular, the zones of slowest-conduction velocity during tachycardia (critical zones) exhibited very slow conduction during sinus rhythm.
2. The critical zones were often common to multiple VT morphologies in the same heart. Thus, these

areas can support tachycardias of different configurations, cycle length, and exit sites serving as “anchor” points for multiple VT morphologies.

3. The VT critical zones consistently occurred in areas with very low voltage (≤ 0.55 mV) and SAGs during sinus rhythm.
4. Low voltage or late potentials are not specific for isthmus sites including common anchor sites, probably because dead-end pathways may exist that do not contribute consistently to the main circuits.

RELATIONSHIP BETWEEN THE VT ISTHMUS AND CONDUCTION PROPERTIES DURING SINUS RHYTHM

The primary finding of this study is the strong correlation between conduction properties during sinus rhythm and isthmus sites during tachycardia. Areas with SAG during sinus rhythm corresponded to isthmus sites during tachycardia, and those areas with the most significant activation gradients during sinus rhythm corresponded to critical zones that were common to multiple tachycardia configurations. SAGs during sinus rhythm were more sensitive, specific, and predictive of isthmus sites compared with voltage and EGM criteria. The PPV of conduction velocity slowing $\geq 75\%$ during sinus rhythm for critical zones was 70% (68.8% to 74.6%). This predictive value is significantly higher than voltage abnormality (21%; 17.7% to 25.3%) or isolated late potentials 16% (13.6% to 19.1%). In particular, areas with SAG during sinus rhythm represented zones vulnerable for conduction slowing or block also during re-entry. These re-entry-vulnerable zones may represent physiologically relevant targets for selective ablation. **Figure 8** describes this novel concept of mapping the re-entry-vulnerable zones. Note that the zone with SAG during sinus rhythm is significantly smaller than the low-voltage zone, and this area can support multiple VT morphologies and configurations. In particular, the combination of SAG with very low bipolar voltage amplitude could be a surrogate for critical-zone sites.

The relationship between conduction gradients during sinus rhythm and isthmus sites during VT was first reported by Ciaccio et al. (17) in a canine model of healed infarction. In this elegant study, the authors reported that isthmuses of different VTs were centered around common sites or “anchors” exhibiting marked conduction slowing or SAGs during sinus rhythm. Interestingly, EGMs during sinus rhythm at these anchor locations were relatively short, rather than fractionated or late. This is because areas with

SAGs during sinus rhythm reflect a dynamic condition, whereas isolated late potentials often represent dead-end pathways remote from the re-entrant circuits. The relationship between conduction properties during sinus rhythm and the VT isthmus was also reported by Irie *et al.* (27). The authors retrospectively analyzed properties of conduction during sinus rhythm in patients with scar-related VT who underwent ablation. They found that areas of slow conduction during sinus rhythm were more predictive for VT termination sites than the zones of latest activation.

MULTIPLE VT MORPHOLOGIES SHARE COMMON SITES WITH SAG DURING SINUS RHYTHM

In this study, we found that multiple VT morphologies (exit sites, cycle length, and configurations) often shared common elements, centered around areas with SAGs during sinus rhythm. These areas had very low voltage amplitude and served as “anchors” for slow conduction or block supporting re-entry. This observation is consistent with previous reports. Costeas and Wit (28) were the first to report the mechanism of multiple VT morphologies. They reported that, in a canine model of infarction, tachycardias with multiple morphologies commonly arise from re-entrant circuits in the same region of the infarct, suggesting that most often only 1 area has the electrophysiological properties necessary to sustain reentry (28). De Bakker *et al.* (29) used an endocardial multielectrode balloon during VT surgery to map 32 patients with anterior infarction and aneurysm. They found that different tachycardias originated from within a limited area in the scar. Similarly, Miller *et al.* (30) also reported that, in the majority of patients with infarction, multiple VT configurations appeared to originate in the same or adjacent sites (82%; 60 of 73 patients).

RELATIONSHIP BETWEEN THE VT ISTHMUS AND SINUS RHYTHM EGMs

Substrate mapping techniques during sinus rhythm have been developed to identify the VT isthmus in patients in whom the VT is not hemodynamically tolerated or cannot be induced. These techniques are based on observations initially made during open-heart surgery for infarct-related VT. The isthmus of these VTs often corresponded to areas of low voltage and abnormal fractionated or late EGM during sinus rhythm (5). Miller *et al.* (31) demonstrated that surgical removal of these EGMs by subendocardial

resection is an effective therapy for VT, thus implicating these EGMs as the substrate for VT in patients with healed infarction. This initial experience spurred promise and laid the ground for substrate-guided VT ablation during sinus or paced rhythms. However, the excellent results of subendocardial resection surgery have not been reproduced by catheter ablation (10,13,32). This difference in clinical outcome between subendocardial resection and catheter ablation may be attributed to any of these factors: 1) radio-frequency energy may not be powerful enough to eliminate the arrhythmogenic substrate; 2) voltage and EGM abnormalities during sinus rhythm may not have adequate specificity to locate the VT isthmus; 3) patients treated by subendocardial resection during the pre-revascularization era may have had different substrates compared with those treated today, and in particular, patients with partially revascularized tissue tend to have smaller infarcts and border zone, supporting smaller and faster circuits that may extend beyond the subendocardium; and 4) ablation by itself may promote arrhythmia caused by additional scarring and slow conduction.

Cassidy *et al.* (1) analyzed the sinus rhythm EGMs in 52 patients with 102 VT morphologies undergoing mapping during VT and sinus rhythm before subendocardial resection. They found that although abnormal EGMs were present in 86% of VT isthmuses during sinus rhythm, these were also commonly recorded in nonisthmus sites with an overall specificity of 48%. Late potentials, in particular, were recorded in only 26% of isthmuses and carried a modest PPV value of 33% for isthmus sites. These mapping studies were performed using quadripolar nonsteerable catheters with 2-mm tip, 1-mm ring, and 5-mm interelectrode spacing. Our study using cutting-edge technology and detailed mapping during sinus rhythm demonstrated that low-voltage and abnormal EGMs remain relatively nonspecific predictors for the VT isthmus. Whereas isthmus sites were largely confined to low-voltage areas, 17.8% of isthmuses also included areas with normal voltage amplitude. Isolated late potentials were similarly infrequent in isthmus sites (28%) and carried an overall PPV of 32.0%. LAVA was the most common EGM abnormality in isthmus sites (84%). However, these were also common in nonisthmus sites, with PPVs of 31%. These data suggest that voltage and EGM abnormalities during sinus rhythm show limited specificity for isthmus sites, independent of the mapping resolution or technology. However, although EGMs during sinus rhythm are nonspecific for VT isthmus sites, it is possible that EGMs recorded using pacing protocols (different wavefronts and coupling intervals) may be

able to “stress” the conduction system and unmask those areas harboring areas vulnerable for re-entry. Those areas may exhibit cycle length dependence and propensity to propagation block in a fashion similar to the atrioventricular conduction system to identify the presence of a slow pathway (33).

STUDY LIMITATIONS. This study was performed in swine and used an established human-like model of subendocardial infarction and VT; however, it requires validation in humans and particularly in patients with other than anterior-wall infarction. This study examined the correlation between hemodynamically tolerated VTs and the corresponding conduction properties during sinus rhythm. However, circuit characteristics of faster nontolerated VT may be more complex, with a larger component of functional block not present during sinus rhythm. In this regard, these data cannot be extended to patients with non-infarct-related substrate with intramural involvement that cannot be mapped using available technologies.

CONCLUSIONS

This study reports a novel method to specifically identify the VT isthmus during sinus rhythm. The recent availability of newer mapping technologies provides sufficient resolution to incorporate functional elements, including local conduction velocity,

to identify those zones vulnerable for re-entry. This physiological approach may allow delivery of focused ablation (either via catheters or extracorporeal radiation) to the critical arrhythmogenic substrate.

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PERSPECTIVES

COMPETENCY IN MEDICAL KNOWLEDGE: The VT isthmus corresponds to sites with SAGs during sinus rhythm. These sites exhibit very low voltage amplitude and can support tachycardias of different morphologies in the same heart. It allows for identification of re-entry anchors with high sensitivity and specificity.

TRANSLATIONAL OUTLOOK: New high-resolution mapping technologies and algorithms can identify areas with SAGs during sinus rhythm. These areas are vulnerable for re-entry and may represent new and more specific targets for ablation.

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APPENDIX For an expanded Methods section as well as supplemental figures and videos, please see the online version of this paper.



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